

EXPERIMENTAL DETERMINATIONS OF THE ROUND REACTION FORCE DEPENDING ON THE CHARACTERISTICS OF SOLE MATERIALS AND GROUND SURFACE

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Abstract: Forța de reacțiune a solului ocupă un loc important în contextul general al analizei mișcării umane. Reacția corpului la modificările încălțăminte – fie ele modificări și insertii ale încălțăminte, fie corecții ortopedice ale piciorului – depinde de intervalul de timp în care se utilizează un anumit tip de încălțăminte. De fapt, efectele biomecanice ale modificărilor încălțăminte trebuie să fie diferențiate în funcție de timpul necesar pentru adaptarea corpului la aceste modificări.

Scopul acestui studiu a fost de a determina forța de reacțiune a solului în funcție de caracteristicile materialelor utilizate pentru talpa la mersul normal pe diferite tipuri de suprafețe ale solului.

Ground reaction force occupies an important place in the overall context of human motion analysis. The body's reaction to changes in footwear – whether they are shoe modifications and inserts or orthopedic corrections – depends on the time period within which a particular type of footwear is used. In fact, the biomechanical effects of changes in footwear must be differentiated according to the time needed for the body to adapt to these changes.

The purpose of this study was to determine the ground reaction force depending on the characteristics of the materials used for the sole in normal gait on different types of ground surfaces.

Keywords: Ground reaction, Force plate, Biomechanics, Footwear

1. Introduction

Research conducted in recent decades on the ground reaction force during walking has examined how these forces affect the body and the factors that influence them, such as style of walking, stepping surfaces and footwear type. It was found that the body is subjected to dynamic forces 1.1 to 1.3 times the body weight while walking. Also, the role of footwear in sports activities was studied in order to reduce stress, avoid the foot injuries, and to improve performances. It

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must be taken into account that the feet are among the most stressed body parts and that they unfortunately receive only a small part of our daily attention. This is why a lot of people find, sometimes too late, that they have a number of health problems in their feet.

Shoes that do not provide adequate support can lead to an imbalance of the whole body. Proper footwear commands static and dynamic balance of feet, and consequently, a correct center of gravity shift, resulting in balancing the whole body.

Increased interest in studying human movement required to design and develop techniques and equipment to record it. These have enabled to analyze the movement in terms of quality (appearance of movement) or quantity (speed, acceleration, force), significantly contributing to the understanding of basic mechanisms underlying human motion.

Of the kinetic-dynamic parameters that characterize human gait, ground reaction force is of particular relevance. Studies have already established the approximate shape of the variation curve during walking, specific for its components and whose parameters vary from individual to individual, body weight also playing an important role.

Measurement of ground reaction is carried out using force plates. Force plates have been used since the late 1890s. Initially, force platforms were used to measure the vertical component of ground reaction force (GRF). Since 1970, the GRF data obtained have been used to determine the forces acting on the body during walking. Mitigating the dynamic ground reaction force is a constant concern in the manufacture of footwear.

The purpose of this study is to compare the horizontal components of ground reaction force for various kinds of shoes with soles made of different materials, on different types of ground surfaces. The test was attended by volunteers using the same types of shoes on the same types of surfaces. The types of shoes used were: sandals, shoes, leisure shoes, and boots.

2. Experimental

2.1 Equipment

Force determination was carried out using an AMTI force plate and a plate made at the Faculty of Mechatronics and Precision Mechanics of “Politehnica” University of Bucharest (UPB).

The AMTI’s AccuGait System force plate presented in (Fig. 1) was set up in a special walking track. It should be noted that the force plate system of use includes hardware, the analogue / digital converter and data analysis software entitled AccuGait, using NetForce and NetForce / BioAnalysis components.



Fig. 1. AMTI force plate

Each analysis module is designed and developed to provide an integrated, unique solution, for biomechanical analysis activities. Bioanalysis comes with a set of graphic tools.

Graphic bioanalysis shows various parameters of gait, balance and power which are most commonly used in the field, namely: F_x , F_y , F_z , GRF in 3D, the center of pressure, M_x , M_y , M_z moments.

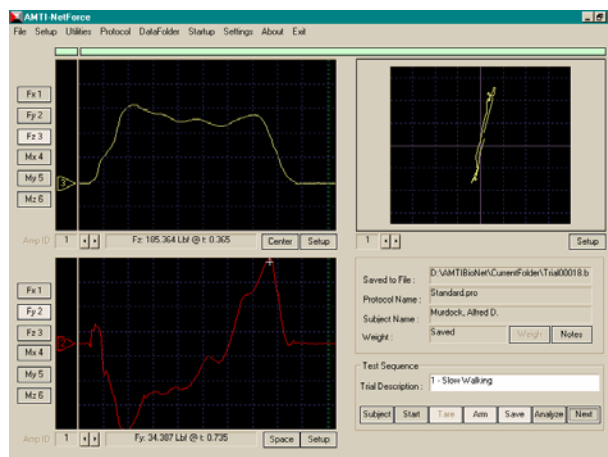


Fig. 2. Display of obtained experimental data

The force plate made by UPB is presented in (Fig. 3)

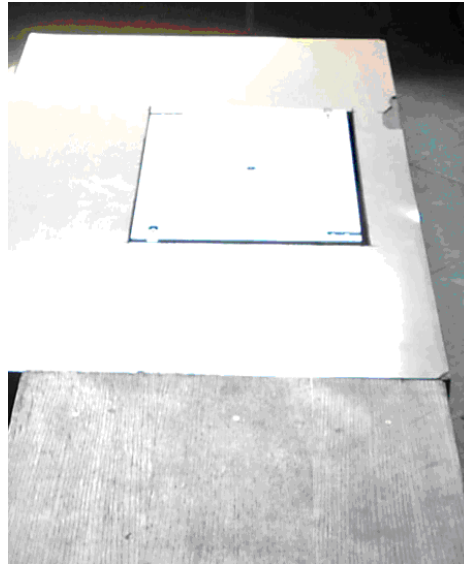


Fig. 3. Force plate made at UPB.

This plate allows simultaneous measurement of the three components of ground reaction force (Fig.4).

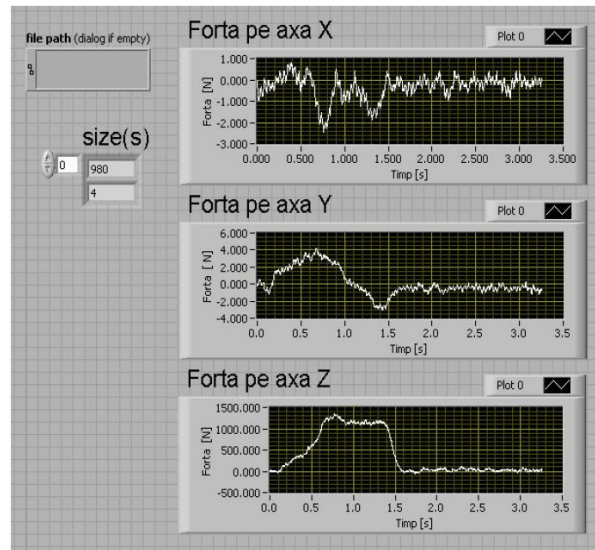


Fig. 4. Display of obtained experimental data

2.2 Subjects

Three healthy female volunteers aged $50 \div 52$, weighing $69 \div 72$ kg have participated in the tests. They have expressed their consent prior to participating in this experiment.

2.3 Procedure

Subjects walked on the track where the force plate was introduced, each wearing seven different kinds of shoes. Walking was done on seven different areas applied on the platform. Only studies in which the right foot landed fully on the plate were valid. The analyzed shoes had different heel heights, ranging from 0.5 to 7 cm, width between 2 and 6 cm, made of various materials: polyurethane, rubber, PVC, ABS. Walking surfaces used in the study were as follows: metal, linoleum, parquet, carpet, rubber, asphalt, stone tile.

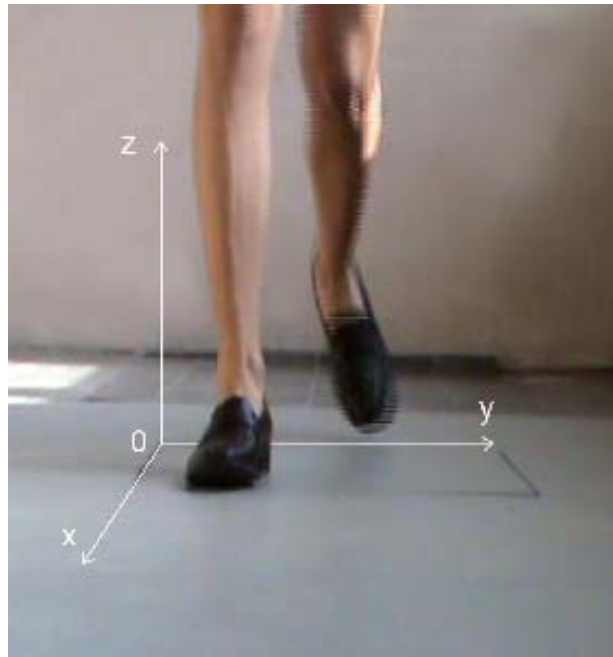


Fig. 5. Manner of stepping on the force plate

3. Results

Ground reaction force is dependent on the mechanical properties (stiffness, adhesion, etc.) of the contact surfaces (in our case shoe soles and support surface). The role of the stepping surface during walking is that of braking, supporting, and pushing.

From the data recorded on the force platform the maxima of the three ground reaction force components were chosen for analysis, namely, the vertical component F_z , the anteroposterior component F_x , and the medio-lateral component F_y .

When there is heel contact between the foot and the floor, the force is zero, as heel strike is defined when contact is generated. In a very short period of time, after heel strike, the force begins to increase rapidly, as the body is supported by the foot. Due to the fact that the center of mass shifts down and with some deceleration, the inertial force must be added to the gravitational force, which means that the vertical force applied through the foot exceeds body weight and reaches the peak, which can be seen in Fig. 6.

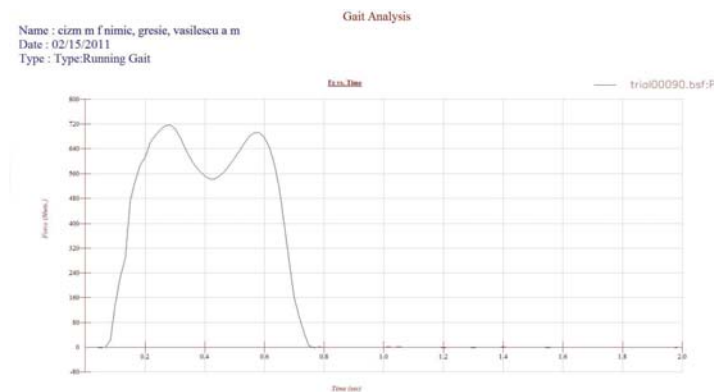


Fig.6. Variation of the F_z vertical component of the ground reaction during normal gait.

During unipodal support, when the heel contacts the ground, there is a rapid deceleration which leads to an increase of ground reaction force which exceeds body weight. Then, the center of mass undergoes a downward acceleration, which will produce an inertial force directed upwards, which will reduce the ground reaction force. When the human body is upright, the vertical component of ground reaction force is equal to the weight of the human body.

In the final stage of the support phase (propulsion) the propulsive action generates greater forces than body weight. The second peak occurs about mid-cycle during walking. As the limb is ready for lift-off, the force quickly reaches zero at the end of support phase.

In the second half of unipodal phase support, in order to accelerate the body's center of mass forward, the ground applies a forward directed force on the foot. This occurs as a gradual and then rapid increase, followed by a rapid reduction of force.

Anteroposterior reaction force F_x is the horizontal force exerted by the force plate on the foot (Fig. 7), acting in the walking direction of the subject with a lower magnitude than the vertical ground force component of the soil. At first there is a braking force in the mid-stance phase, with the purpose of reducing the speed of the body's center of mass which is then followed by propulsion. Close to the mid-stance phase, F_x becomes positive, which means that the force plate reaction acts forward, while muscle forces push the foot on the plate.

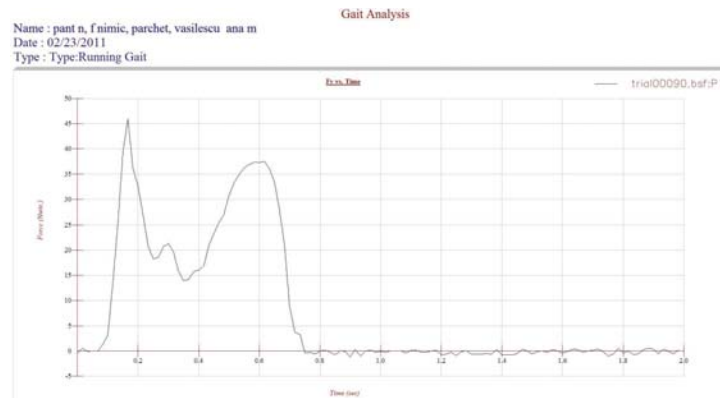


Fig.7. Variation of anteroposterior component F_x of ground reaction force during normal gait

The horizontal component perpendicular to walking direction F_y (Fig. 8) is due to oscillations in the frontal plane with an important role in providing balance in the unipodal support phase. For this, the size of the area of contact with the ground is relevant (for example, walking in high heels, where foot oscillations in the frontal plane are very pronounced).

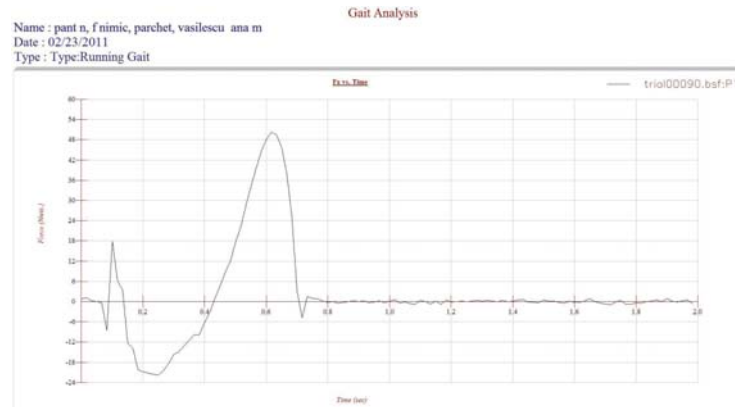


Fig.8. Variation of mediolateral component F_y of ground reaction force during normal gait

Table 1 presents values of the F_z , F_y , F_x components of the ground reaction for shoe sole materials (levicel, polyurethane, leather, thermoplastic rubber, polyvinyl chloride, durocol, dermadur) on contact surfaces (metal, carpet, linoleum, parquet, rubber, asphalt, stone tile) for the two subjects. Subject 1 weighs 72 kg and subject 2 69 kg. The angle between the vertical component F_z and the medio-transverse component F_y was also calculated.

Table 1

Values of ground reaction components

| Sole material – contact surface | Fz(N) maximum | | Fy(N) maximum | | Fx(N) maximum | | Angle between Fz and Fy (°) | |
|---------------------------------|----------------|----------------|----------------|----------------|----------------|----------------|-----------------------------|----------------|
| | A ¹ | B ² | A ¹ | B ² | A ¹ | B ² | A ¹ | B ² |
| levicel-metal | 715 | 694 | 24 | 24 | 82 | 82 | 1,92 | 1,98 |
| levicel-carpet | 719 | 694 | 25 | 26 | 82 | 74 | 1,99 | 2,14 |
| levicel-linoleum | 736 | 690 | 16 | 20 | 82 | 82 | 1,24 | 1,66 |
| levicel-parquet | 736 | 715 | 24 | 24 | 98 | 90 | 1,87 | 1,92 |
| levicel-rubber | 722 | 720 | 25 | 28 | 102 | 74 | 1,98 | 2,22 |
| levicel-asphalt | 736 | 694 | 24 | 24 | 82 | 82 | 1,86 | 1,98 |
| levicel-stone tile | 736 | 715 | 24 | 24 | 96 | 90 | 1,86 | 1,92 |
| PU-metal | 715 | 694 | 16 | 32 | 65 | 82 | 1,28 | 2,64 |
| PU- carpet | 715 | 694 | 24 | 32 | 82 | 74 | 0,033 | 0,046 |
| PU- linoleum | 726 | 715 | 24 | 16 | 82 | 82 | 0,033 | 0,022 |
| PU- parquet | 715 | 736 | 24 | 24 | 82 | 90 | 0,033 | 0,032 |

| | | | | | | | | |
|----------------------|-----|-----|----|----|-----|-----|-------|-------|
| PU-rubber | 718 | 732 | 16 | 24 | 65 | 80 | 0,022 | 0,032 |
| PU-asphalt | 736 | 694 | 24 | 16 | 82 | 82 | 0,032 | 0,023 |
| PU-stone tile | 715 | 694 | 24 | 24 | 90 | 90 | 0,033 | 0,034 |
| leather -metal | 736 | 725 | 16 | 22 | 106 | 89 | 0,021 | 0,030 |
| leather - carpet | 700 | 694 | 16 | 16 | 99 | 74 | 0,022 | 0,023 |
| leather -linoleum | 715 | 673 | 16 | 16 | 90 | 90 | 0,022 | 0,023 |
| leather - parquet | 736 | 736 | 24 | 24 | 98 | 98 | 0,032 | 0,032 |
| leather -rubber | 709 | 719 | 30 | 17 | 117 | 101 | 0,042 | 0,023 |
| leather -asphalt | 748 | 694 | 24 | 16 | 88 | 90 | 0,032 | 0,023 |
| leather - stone tile | 736 | 736 | 24 | 24 | 98 | 98 | 0,032 | 0,032 |
| TR-metal | 733 | 724 | 32 | 24 | 101 | 97 | 0,043 | 0,033 |
| TR- carpet | 752 | 724 | 22 | 14 | 101 | 97 | 0,029 | 0,031 |
| TR- linoleum | 742 | 717 | 30 | 21 | 112 | 102 | 0,040 | 0,029 |
| TR- parquet | 730 | 705 | 28 | 22 | 86 | 93 | 0,030 | 0,031 |
| TR- rubber | 709 | 719 | 30 | 17 | 117 | 101 | 0,042 | 0,023 |
| TR-asphalt | 705 | 730 | 24 | 25 | 110 | 90 | 0,034 | 0,034 |
| TR- stone tile | 712 | 716 | 29 | 16 | 86 | 99 | 0,040 | 0,022 |
| PVC-metal | 700 | 727 | 19 | 13 | 127 | 83 | 0,027 | 0,017 |
| PVC-carpet | 718 | 717 | 15 | 19 | 118 | 97 | 0,020 | 0,026 |
| PVC-linoleum | 714 | 718 | 25 | 13 | 116 | 100 | 0,022 | 0,023 |
| PVC- parquet | 729 | 729 | 23 | 16 | 111 | 104 | 0,035 | 0,021 |
| PVC-rubber | 759 | 713 | 21 | 17 | 133 | 93 | 0,027 | 0,023 |
| PVC-asphalt | 759 | 722 | 28 | 23 | 112 | 102 | 0,036 | 0,031 |
| PVC- stone tile | 700 | 703 | 14 | 22 | 109 | 74 | 0,020 | 0,031 |
| durocol-metal | 730 | 715 | 20 | 15 | 127 | 98 | 0,027 | 0,020 |
| durocol- carpet | 726 | 697 | 22 | 18 | 121 | 80 | 0,030 | 0,025 |
| durocol-linoleum | 719 | 716 | 25 | 19 | 123 | 89 | 0,034 | 0,026 |
| durocol- parquet | 722 | 737 | 26 | 27 | 137 | 101 | 0,036 | 0,036 |
| durocol-rubber | 722 | 713 | 25 | 22 | 122 | 92 | 0,034 | 0,030 |
| durocol-asphalt | 701 | 716 | 26 | 17 | 107 | 82 | 0,037 | 0,023 |
| durocol-stone tile | 700 | 722 | 18 | 24 | 99 | 86 | 0,025 | 0,033 |
| dermadur-metal | 733 | 722 | 41 | 45 | 146 | 86 | 0,055 | 0,055 |
| dermadur-carpet | 743 | 704 | 30 | 35 | 102 | 102 | 0,040 | 0,049 |
| dermadur-linoleum | 726 | 705 | 31 | 31 | 113 | 92 | 0,042 | 0,043 |
| dermadur-parquet | 755 | 697 | 40 | 36 | 113 | 95 | 0,052 | 0,051 |
| dermadur-rubber | 739 | 708 | 35 | 40 | 103 | 99 | 0,047 | 0,056 |
| dermadur-asphalt | 724 | 722 | 29 | 26 | 105 | 101 | 0,040 | 0,036 |
| dermadur-stone tile | 718 | 699 | 18 | 39 | 102 | 89 | 0,025 | 0,055 |

4. Conclusions

A first conclusion was that the indications of the two plates were very close, which makes the UPB plate more advantageous due to its much lower price.

Tests conducted on the force plates have revealed that the values of ground reaction force components in the three directions (F_z , F_y , F_x) for two subjects of similar weight, wearing the same shoes and walking on the same contact surface are different due to their different walking style.

Values of GRF components vary depending also on the nature of the sole material, and the type of ground surface.

Foot and shoe form an assembly whose characteristics are specific to each individual, and the recommendation is to make custom footwear.

In conclusion, the wrong footwear design and construction leads to additional correction efforts of the whole body.

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